

# Influence of Microtextured Implant Surfaces on Peri-implantitis and Its Treatment: A Preclinical Trial

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**Purpose:** The prevalence of peri-implantitis has increased significantly, forcing clinicians to search for ways to prevent it. Laser-microtextured surfaces promote soft tissue attachment and provide a tight seal around implants. Hence, the aim of this study was to examine the clinical, radiographic, and histologic features of ligature-induced peri-implantitis, as well as the effect of surgical treatment of these induced peri-implantitis lesions on laser-microtextured implants in a controlled animal model. **Materials and Methods:** Six mini-pigs (three males/three females) received 6 implants each (3 resorbable blast textured [RBT] implants and 3 laser-microtextured [LM] implants) in mandibular premolar sites, for a total of 36 implants. Two groups were identified based on the time point of sample analysis. After osseointegration was achieved, metal wire ligatures were placed and left for 12 weeks. Group 1 samples were then obtained, and group 2 samples received rescue therapy following a guided bone regeneration (GBR) protocol. Sample collection in group 2 was completed 12 weeks after the samples were submerged and treated. All samples were analyzed histologically and measurements were taken. **Results:** Four implants (three RBT, one LM) were lost at early time points because of implant instability. Interimplant distances and soft tissue thicknesses varied subtly between groups. More notable was the mean ( $\pm$  standard error of the mean) crestal bone loss (group 1: 1.860  $\pm$  1.618 mm [LM] and 2.440  $\pm$  2.691 mm [RBT]; group 2: 2.04  $\pm$  1.613 mm [LM] and 3.00  $\pm$  2.196 mm [RBT]) ( $P < .05$ ), as demonstrated by a paired t test. Histologic pocket depth was also greater at RBT sites than at LM sites (4.448  $\pm$  2.839 mm and 4.121  $\pm$  2.251 mm, respectively, in group 1; and 3.537  $\pm$  2.719 mm and 2.339  $\pm$  1.852 mm, respectively [ $P < .005$ ] in group 2). **Conclusion:** LM implants had less crestal bone loss and shallower histologic pocket depth compared with their RBT counterparts. Also, LM implants had higher bone fill when a rescue therapy (GBR) was performed. INT J ORAL MAXILLOFAC IMPLANTS 2017 (7 pages). doi: 10.11607/jomi.5599

**Keywords:** implant surface, microtextured implant surface, peri-implantitis

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Osseointegrated endosseous dental implants for replacement of lost dentition have been in use for more than 30 years with widely reported success.<sup>1-4</sup> However, this journey has not been without complications. The increasing numbers of dental implants placed have led to more implant-related complications, which create a challenging and an unpredictable burden for patients and dentists alike. Several attempts have been made to define the diseases associated with dental implants, and two main entities have emerged: peri-implant mucositis and peri-implantitis.<sup>2,5-7</sup> Peri-implant mucositis is the presence of inflammation in the mucosa at an implant site with no signs of loss of supporting bone beyond the initial physiologic bone remodeling.<sup>8</sup> In addition to inflammation in the mucosa, peri-implantitis is characterized by loss of supporting bone beyond the initial biologic bone remodeling.<sup>8</sup> Derks et al<sup>4</sup> reported a peri-implantitis prevalence ranging from 28% to 56% of subjects and 12% to 43% of implant sites, which ultimately leads to a total implant loss of 7.6%. This variation in prevalence could be due largely to the lack of uniformity in criteria used to define peri-implantitis, as well as to the variables inherent in the diagnosis of disease.<sup>9,10</sup> Because of the high incidence of peri-implant complications,

practitioners have tried several surgical and nonsurgical treatments, concluding that peri-implant mucositis is treatable with nonsurgical therapy; however, peri-implantitis seems to respond better to surgery, but the results are unpredictable.<sup>5,11,12</sup> In the absence of a safe and predictable treatment for peri-implantitis, the focus on prevention has become even more important.

Several factors influence the incidence of peri-implantitis; patient-based risk indicators include, but are not limited to, poor-oral hygiene, smoking, alcohol consumption, history of periodontitis, diabetes mellitus, and genetic traits. Factors leading to early implant loss include smoking, history of periodontitis, implant length less than 10 mm, and certain implant surface characteristics, with the last factor being especially relevant to late implant loss.<sup>4</sup> Other determining factors for crestal bone loss and peri-implantitis are implant macrodesign and surface treatments.<sup>4,7</sup> The Seventh European Workshop on Periodontology examined whether implant surfaces play a role in the etiology of peri-implant diseases.<sup>5</sup> A review by Renvert et al<sup>13</sup> revealed that while clinical evidence was lacking with regard to the effect of implant surfaces on the initiation of peri-implantitis, limited experimental evidence showed that surface characteristics may have an effect on the progression of established peri-implantitis.

Recent animal studies have shown that a difference exists in the extent of experimentally induced peri-implantitis between different rough surfaces.<sup>14–16</sup> The researchers found that certain rough surfaces were associated with greater bone loss with spontaneous progression of peri-implantitis. This disease progression is likely to occur if an invasion of pathogenic bacteria and chronic inflammation occur through the gingival sulcus due to failure of the soft tissue seal. Consequently, there has been a growing focus on optimizing the transmucosal component of dental implants in hopes of promoting mucosal and connective tissue (CT) attachment and, hence, creating a resistant seal to the oral cavity. To accomplish this, laser-etched microgrooved titanium surfaces have been used to promote the contact guidance phenomenon, which refers to the tendency of a cell to be oriented and guided in its direction of motion by the shape of the surface with which it is in contact.<sup>17</sup>

Depending on the groove characteristics (depth, width, pitch), the cell response may vary from a focal adhesion to just the groove ridge to the entire cell's adhering to the groove floor or wall. In vitro and in vivo studies seem to suggest that horizontal grooves on transmucosal components of implants encourage formation of a wider zone of CT attachment<sup>18</sup> and prevent epithelial downgrowth.<sup>19,20</sup>

Laser-microtextured titanium surfaces (Laser-Lok, BioHorizons) that promote soft tissue attachment to implant structures are a promising advancement in the field of implant dentistry. Animal and human evidence of CT attachment to laser-microtextured titanium

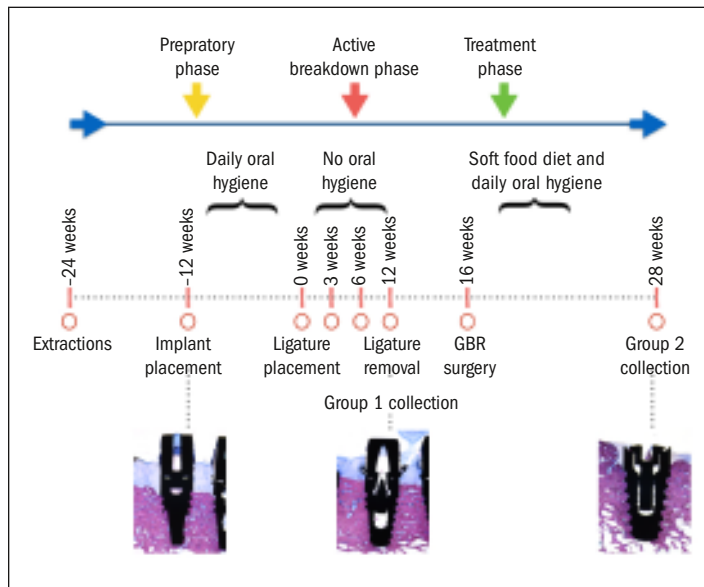
surfaces has been demonstrated at the histologic level after a healing period of 3 and 6 months, respectively.<sup>21,22</sup> To test the endurance of the CT attachment observed around laser-microtextured titanium implants, the authors aimed to study the clinical, radiographic, and histologic features of ligature-induced peri-implantitis at dental implant sites with similar geometry but different surface characteristics of the implant collar. A secondary aim was to evaluate the effect of surgical treatment of experimentally induced peri-implantitis using guided bone regeneration (GBR) on two implant surfaces in a controlled animal model.

## MATERIALS AND METHODS

The Institutional Animal Care and Use Committee of Mississippi State University approved all animal experiments (approval no. 12-050). Six mini-pigs (three male, three female), weighing between 70.3 and 89.4 kg, bred exclusively for biomedical research purposes, were obtained from a licensed vendor and used for the experiments. The authors determined the sample size by performing a power sample size calculation and by considering previous studies with similar sample sizes.<sup>14–16</sup> All surgical procedures were carried out under general anesthesia induced with intravenous propofol (10 mg/mL, 0.6 mL/kg) and sustained with nitrous oxide:oxygen (1:1.5–2) and isoflurane in conjunction with endotracheal intubation.

Endosseous solid screw-type implants (tapered internal system, BioHorizons) were used in this research. Two configurations (resorbable blast textured [RBT] and laser-microtextured [LM]) were used based on the surface texture of the implants. All implants were internal hex, 3.4 mm in diameter and 9 mm in length. RBT implants received standard narrow-profile abutments and LM implants received microtextured narrow-profile abutments.

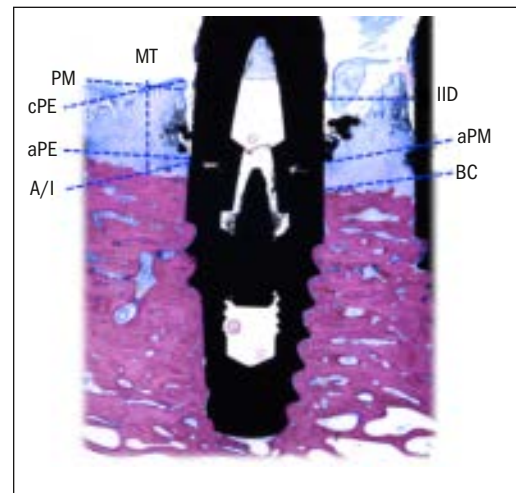
The study was divided into three phases: (1) preparatory phase, (2) active breakdown phase, and (3) treatment phase (Fig 1). Samples in group 1 were obtained after the active breakdown phase, and samples in group 2 were obtained after the treatment phase. During phase 1, mandibular premolars (P2, P3, P4) were extracted and the sites were left to heal under secondary intention for 12 weeks. After the 12-week healing period, a second surgical procedure was performed to place the implants. A mucoperiosteal flap was raised on each lower quadrant, and three RBT or LM implants were placed in an alternating manner according to a randomization code. Hence, each animal received six implants. The healing abutments were placed over each implant, and the flaps were approximated around the abutments and sutured without tension. Sutures were removed at 2 weeks, and animals were switched to a soft-food diet. Phase 2 began 12 weeks after implant surgery; at



**Fig 1** Study timeline depicting the preparatory phase, active breakdown phase, and treatment phase. Oral hygiene protocols and diet are also shown, as well as the sample collection time points and treatment provided.

this point, laser-microtextured healing abutments together with metal ligatures were placed in the peri-implant sulcus of each implant. This step coincided with the end of all oral hygiene procedures to allow for the induction of experimental peri-implantitis. At week 12, animals in group 1 were euthanized using a lethal dose of sodium pentothal. Bone blocks containing the implants were obtained and subjected to histologic analyses. For phase 3 experiments in the remaining three animals (group 2), the ligatures were removed and oral hygiene procedures were reestablished. Four weeks later, surgery was performed; mucoperiosteal flaps were raised to provide access following degranulation and debridement. The implant surfaces were then cleaned with cotton saturated with a tetracycline solution (250 mg diluted with 2.5 mL sterile saline solution). Areas were then irrigated with normal saline. A GBR procedure was performed in which a combination of xenogenic bovine bone (Laddec, BioHorizons) and a collagen membrane (Mem-Lok RCM, BioHorizons) was used to repair the peri-implant defects. Submerged healing took place for 12 weeks, after which the animals were euthanized and the specimens were subjected to histologic analysis. After euthanasia, the jaws were retrieved and placed in the fixative solution; tissue blocks containing the implant and surrounding soft and hard tissues were dissected using a diamond saw (Exakt, Kulzer) and processed for ground sectioning according to standard protocol.<sup>23</sup> Sections were stained with hematoxylin-eosin and toluidine-azure II and examined using both stereomicroscopy and light microscopy.

Figure 2 shows the landmarks identified and used for the linear measurements (ImageJ software, National Institutes of Health). A masked examiner (JCR) made all linear measurements by setting known parameters and performing triplicate measurements on the mesial and distal aspects of each implant. Measurements were based on the marginal position of the peri-implant mucosa (PM), the abutment-fixture (A/F) junction, the



**Fig 2** Demarcation of anatomical landmarks used for measurements on the implant histologic sample: PM = marginal peri-implant mucosa; aPM = apical plaque margin; MT = mucosa thickness; A/I = abutment-implant junction; cPE = coronal pocket epithelium; aPE = apical pocket epithelium; IID = interimplant distance; BC = bone crest.

**Table 1** Bone Loss (mm) from the Abutment-Fixture Junction to the Bone Crest<sup>a</sup>

	Group 1		Group 2	
	LM	RBT	LM	RBT
	1.509	2.463	2.421	3.104
	1.434	1.565	1.614	2.520
	2.244	0.984	1.614	2.370
	2.561	1.122	1.242	2.524
	2.446	2.764	0.535	2.667
	1.839	2.201	1.524	3.275
	2.133	2.183	3.260	1.180
	1.949	2.684	2.187	1.211
	0.989	0.750	1.040	2.088
	1.529	1.283	2.586	2.459
	0.242	5.131	1.559	2.677
	0.348	4.210	2.179	3.766
	2.801	3.939	2.508	3.897
	3.047	2.750	2.486	4.027
	2.140	2.987	3.653	5.196
	2.554	2.037	2.237	5.048
Mean	1.86	2.44	2.04	3.00

<sup>a</sup>Pooled data for mesial and distal implant sites. LM = laser microtextured; RBT = resorbable blast textured.

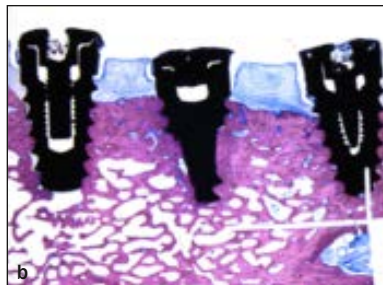
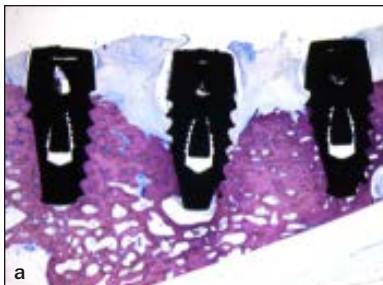
bone crest (BC), the most coronal and apical extension of the pocket epithelium (cPE and aPE, respectively), and the interimplant distance for all sites.

**Table 2 Total Soft Tissue Thickness (mm), Determined in the Interimplant Area with Linear Measurements from Marginal Peri-Implant Mucosa to Bone Crest**

Measurement	Group 1 <sup>a</sup>						Group 2 <sup>b</sup>					
	9086-left	9086-right	9102-left	9102-right	9138-left	9138-right	9089-left	9089-right	9090-left	9090-right	9091-left	9091-right
1	4.263	3.247	2.830	2.693	1.881	3.168	1.657	1.630	0.835	0.657	2.476	1.690
2	4.787	3.591	4.540	2.692	3.282	6.410	0.288	1.139	0.786	1.262	2.157	5.188
3	4.316	3.678	1.489	4.136	3.080	2.960	0.734	0.204	2.719	1.055	2.551	3.610
4	3.542	4.482	4.601	6.624	5.376	3.699	NA	NA	2.526	2.886	3.113	3.084
<b>Mean</b>	4.22	3.74	3.36	4.03	3.40	4.05	0.89	0.99	1.71	1.46	2.57	3.39

<sup>a</sup>Total mean thickness = 3.806 mm.

<sup>b</sup>Total mean thickness = 1.838 mm.



**Fig 3a** Histologic samples in group 1. The mesial and distal implants have a laser-microgrooved (LM) texture, and the middle implant has a resorbable blast textured (RBT) surface. Note the extent of bone loss associated with the middle implant but the higher bone crest level on the mesial and distal sites. Sections were stained with hematoxylin-eosin and toluidine-azure II and examined by means of stereomicroscopy and light microscopy.

**Fig 3b** Histologic samples in group 2. The mesial and distal implants have an RBT surface, while the middle implant has an LM surface. The middle implant has a higher bone crest level than the mesial and distal sites. Sections were stained with hematoxylin-eosin and toluidine-azure II and examined by means of stereomicroscopy and light microscopy.

The measurements included bone loss (A/F to BC), soft tissue thickness at the crestal level (PM to highest BC), histologic sulcus depth (cPE to lowest aPE), and interimplant distance. A paired *t* test was performed as appropriate. Differences were considered significant at  $P < .05$ . Data are presented as mean  $\pm$  standard error of the mean.

## RESULTS

### Clinical Observations

Healing proceeded uneventfully for 32 surgical implant sites during the 12 weeks after extraction of all mandibular premolars and implant placement; 3 RBT and 1 LM implants (9102 middle left, 9089 middle right, 9089 distal left, and 9138 middle right) were lost because of instability at abutment placement. The failures may have been related to premature loading (such as biting the cage). The second phase of the study, after initiation of ligature-induced peri-implantitis, proved uneventful for 12 weeks. The assigned time points were

completed for all animals, and all remaining implants performed well, with no loss or compromised stability.

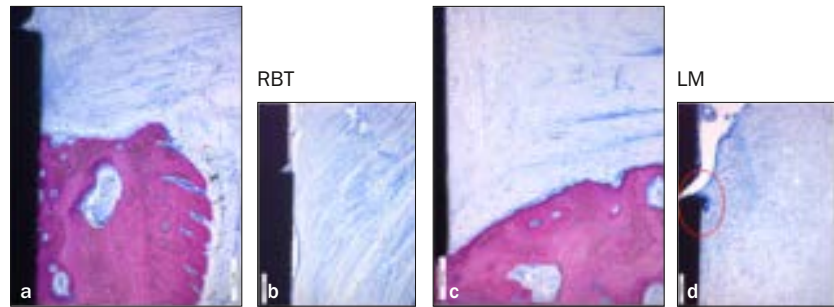
### Histologic Observations

To ensure that unwanted variables were not encountered in the experiments, the authors performed standard measurements of interimplant distances and soft tissue thickness for both groups and implant types. The interimplant distance in both groups was similar (group 1,  $3.451 \pm 1.03$  mm; group 2,  $3.385 \pm 1.445$  mm). This implant location accuracy helped minimize the effect of bone loss in neighboring implant sites (Table 1).

Mean soft tissue thickness in group 1 was  $3.806 \pm 0.441$  mm and in group 2 was  $1.838 \pm 1.501$  mm ( $P < .005$ ) (Table 2). This discrepancy between groups could be attributed to the fact that group 1 had no bone loss at baseline. Similarly, the reduction in soft tissue thickness in group 2 may have been caused by recession and bone loss at the time of treatment and placement of a cover screw.

**Group 1.** Histologic samples are shown in Figs 3 to 5. Both implant systems are shown with ligatures

**Fig 4** Implant-abutment interface area is shown. (a) Dense cellularity associated with resorbable blast textured (RBT) peri-implant tissues compared with (c) laser microgrooved (LM) surface. (b) and (d) Abutment-implant (A/I) junction at higher magnification shows surface characteristics on RBT-treated and LM-treated surfaces. Connective-tissue attachment is seen at the A/I junction on LM surfaces (d) but not on RBT surfaces (b).



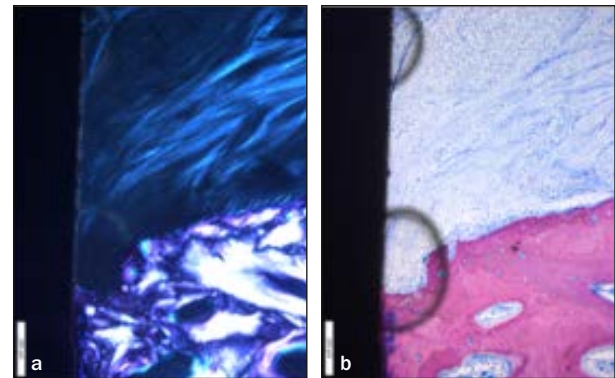
in place; a dense biofilm is seen at the level of the ligatures and migrating apically to the abutment-implant interface. The authors observed a difference between the two implant surface treatments. CT fiber attachment was seen on laser-microgrooved areas in the LM implants, whereas the sulcus of RBT implants seemed to allow a deeper penetration of biofilm and exhibited a higher inflammatory infiltrate (Figs 4 and 5). Different rates of crestal bone loss were observed between samples and among the groups.

**Group 2.** The histologic analysis, performed after completion of regenerative therapy, showed a heterogeneous outcome. In certain cases, the bone-grafted sites experienced an overall reduction in soft tissue support and a greater sulcus depth (Table 3), as well as a slightly increased peri-implant bone loss.

Table 3 shows precise histologic measurements of crestal bone loss. Crestal bone loss in group 1 was  $1.860 \pm 1.618$  mm for LM-treated implants and  $2.440 \pm 2.691$  mm for RBT-treated implants. Slightly higher bone loss was found in both implant types in group 2 (LM implants,  $2.04 \pm 1.613$  mm; RBT implants,  $3.00 \pm 2.196$  mm) ( $P < .005$ ). Histologic pockets were also deeper at RBT sites compared with LM sites ( $4.448 \pm 2.839$  mm and  $4.121 \pm 2.251$  mm, respectively, in group 1;  $3.537 \pm 2.719$  mm and  $2.339 \pm 1.852$  mm, respectively ( $P < .005$ ), in group 2, being statistically significantly different in laser-microtextured implants.

## DISCUSSION

The maintenance of soft tissue contour, characterized by adequate underlying bone, is critical for dental implants placed in esthetically demanding situations.<sup>24,25</sup> Crestal bone remodeling was once believed to be an inevitable process taking place during the first year of implant loading and continuing gradually at a lower scale.<sup>1</sup> Investigators have focused on reducing this remodeling. The introduction of platform switching and laser-modified microtexture at the cervical portion of dental implants has addressed this issue. However, studies have shown that in most scenarios in which these two modalities were tested and compared with



**Figs 5a and 5b** Higher-magnification slides show connective-tissue fiber attachment perpendicular to the laser-microgrooved implant surface in a sample from group 1.

**Table 3** Histologic Pocket Depth (mm) Measured from the Most Coronal and Apical Extension of the Pocket Epithelium

	Group 1		Group 2	
	LM	RBT	LM	RBT
	4.589	5.161	2.474	5.952
	4.071	5.703	2.723	6.256
	2.881	5.523	4.191	3.324
	5.022	7.341	3.115	2.468
	2.799	4.008	2.223	3.358
	2.641	4.616	2.041	3.556
	4.755	3.099	1.624	2.008
	6.372	4.063	1.461	4.061
	1.777	2.360	2.795	3.571
	3.213	3.078	2.660	2.867
	3.947	4.303	2.288	3.426
	4.600	3.889	1.257	1.607
	4.415	6.082	2.634	—
	4.793	3.874	1.271	—
	5.130	4.643	—	—
	4.935	3.437		
Mean	4.121	4.448	2.339	3.537

LM = laser microtextured; RBT = resorbable blast textured.

one another, laser microtexture outperformed platform switching, even in cases involving a thin soft tissue profile.<sup>26–28</sup> In the present study, the LM-treated implants tended to exhibit more resistance to peri-implant tissue inflammation at the breakdown stage. Similarly, once the ligatures were removed, LM-treated implants exhibited less advanced disease progression. These results, based on histologic measurements, also reflect what was observed clinically at the time of sacrifice. Localized inflammation was present in all samples; however, inflammation seemed more severe at RBT implant sites than at LM implant sites, as shown in Fig 3a. Also found was attachment of dense CT fibers with vertical orientation to the implant-abutment interface in the LM-treated implant sites (Fig 3b). Interestingly, because of the study design, lateral sites (mesial or distal) with LM-treated implants tended to limit the amount of bone loss observed in the middle implant site; when LM implants were placed in the middle location, they tended to respond better than their lateral counterparts.

Regarding the study's secondary aim, the GBR procedure proved to be challenging. In all cases the osseous defect left by the ligature-induced experiment was not completely filled. The histologic appearance of the implant types was similar, except for evidence of perpendicular CT fiber attachment on LM surfaces. Consistent with other studies, it was found that application of bone graft and barrier membranes in the treatment of peri-implant defects remains a widely unpredictable approach; however, some level of bone fill was achieved. Similarly, surface treatment resulted in a 1-mm difference in bone gain between groups, favoring the LM surfaces, which, in some cases, reached a 0.5-mm distance from the BC to the implant neck. The results of this study—at both the disease induction phase and the regenerative phase—favored LM surfaces in terms of disease resistance and regenerative potential. The results also support findings in the literature showing multiple benefits of this type of surface modification in maintaining long-term health and esthetics around dental implants.<sup>18,26–28</sup>

Some limitations were also present in this study. Because implants were placed in an intercalated manner, the tissue inflammation from one area tended to extend to the neighboring surface, creating a cumulative inflammatory effect. This was evident histologically, where more crestal bone loss was seen on the implant side exposed to the worst of the three implants. Total bone loss was also reported based on pooled data from mesial and distal aspects to compensate for implant site bias. However, even when these details are taken into consideration, the results clearly favored the LM surface. Also, one must keep in mind that the examiner was masked to the groups.

## CONCLUSIONS

Laser-microtextured implants showed less crestal bone loss after ligature-induced peri-implantitis. They also exhibited higher bone fill when a rescue therapy (GBR) was performed on all implants.

## ACKNOWLEDGMENTS

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